



# MAKING AI MAKE SENSE: CONCEPT-BASED PATHOLOGY DIAGNOSIS AND UNCERTAINTY-AWARE MRI

Asst. Prof. Christian Baumgartner

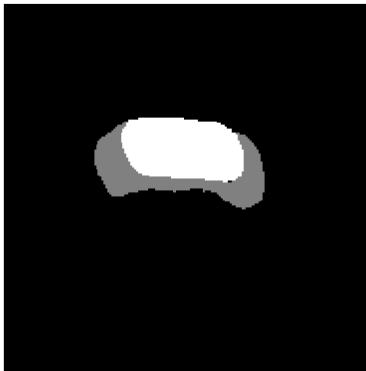
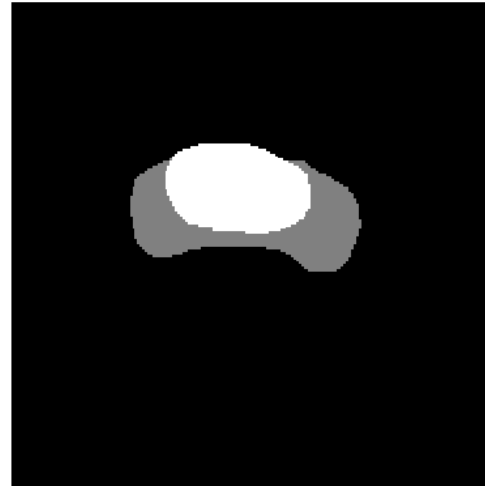




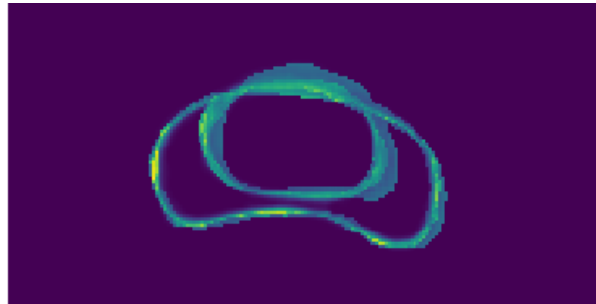
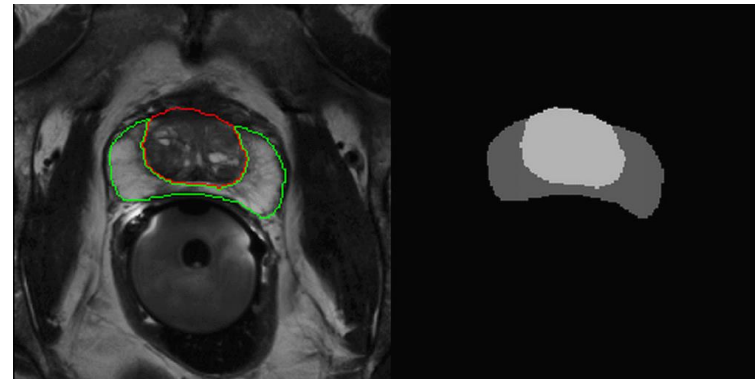
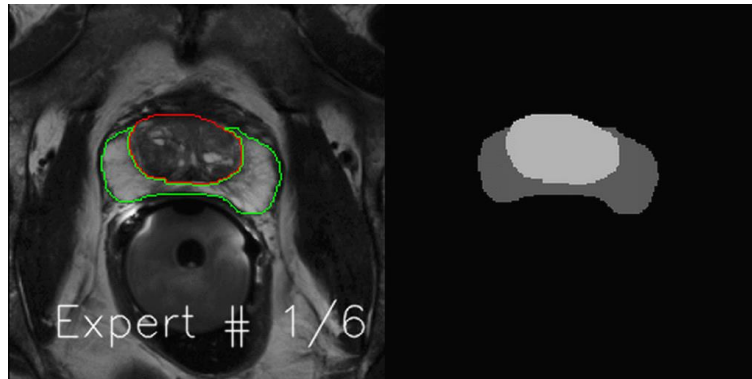
Lucerne Medical AI Group



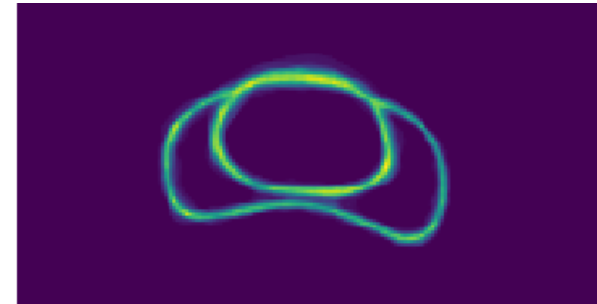
# MEDICAL IMAGING IS FULL OF UNCERTAINTIES



## RESEARCH FOCUS: ESTIMATING UNCERTAINTIES



Annotator variance



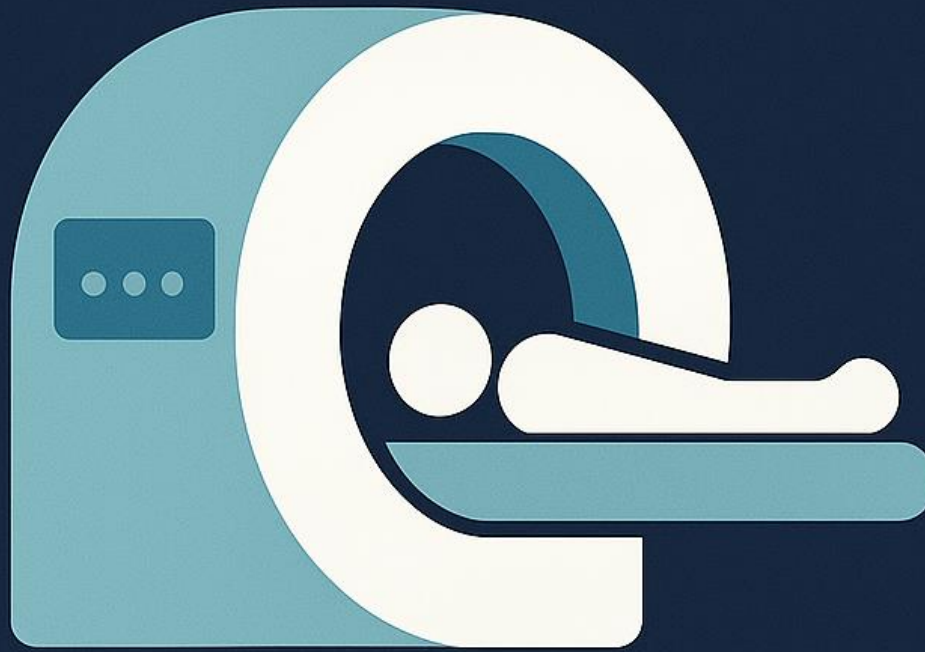
Predicted variance

## RESEARCH GAPS

- 1) Usefulness of uncertainty of regarded as “self-evident”  
→ *Uncertainty is only useful if influences some **downstream** clinical task*
- 2) Clinical decisions of rely on a cascade of clinical steps: how can we propagate uncertainty?



- 3) Could we use uncertainty to do something useful?  
→ Personalise image acquisitions



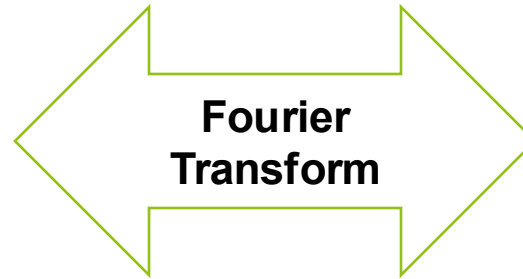
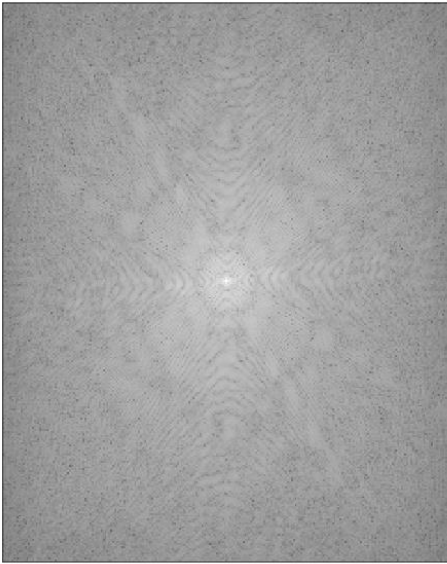
## FAST UNCERTAINTY-GUIDED MR ACQUISITION



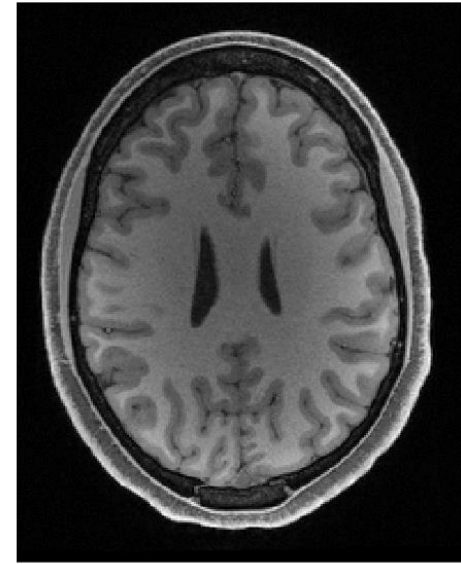
**Paul Fischer**  
PhD Student/  
Post-doc Uni Basel

# QUICK PRIMER ON MRI RECONSTRUCTION

Measurement data (k-space)

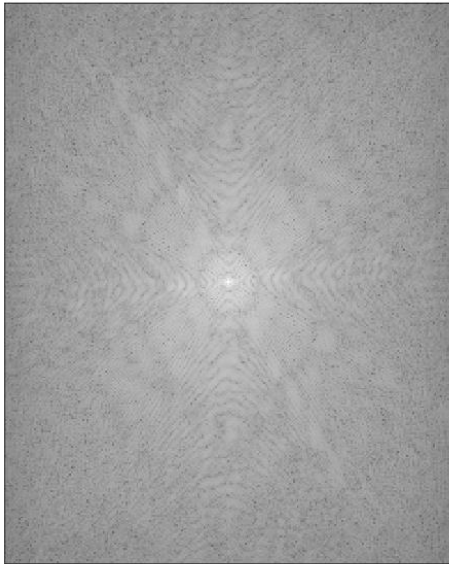


Image

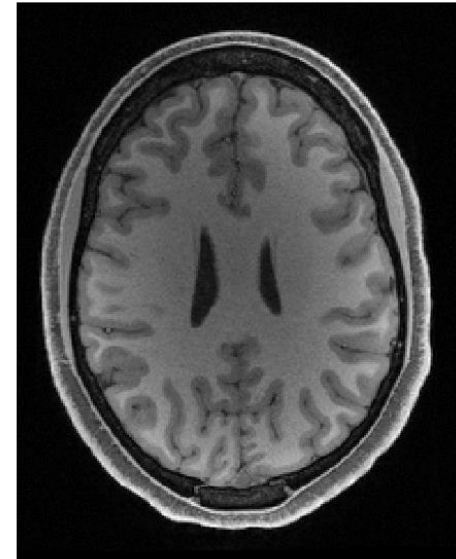


# QUICK PRIMER ON MRI RECONSTRUCTION

Measurement data (k-space)

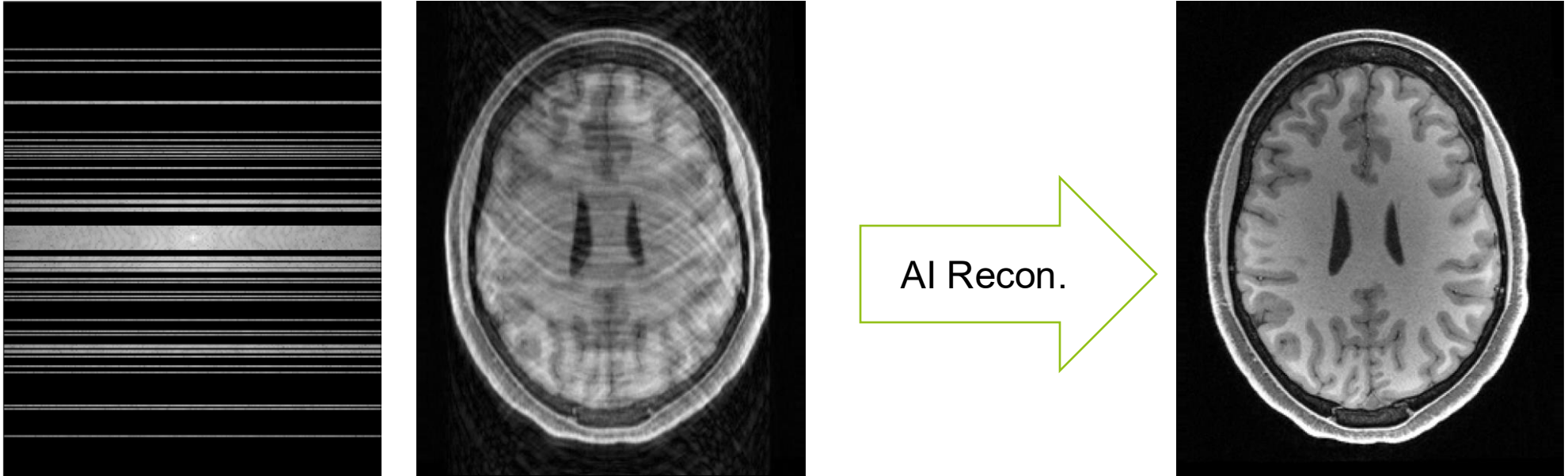


Image





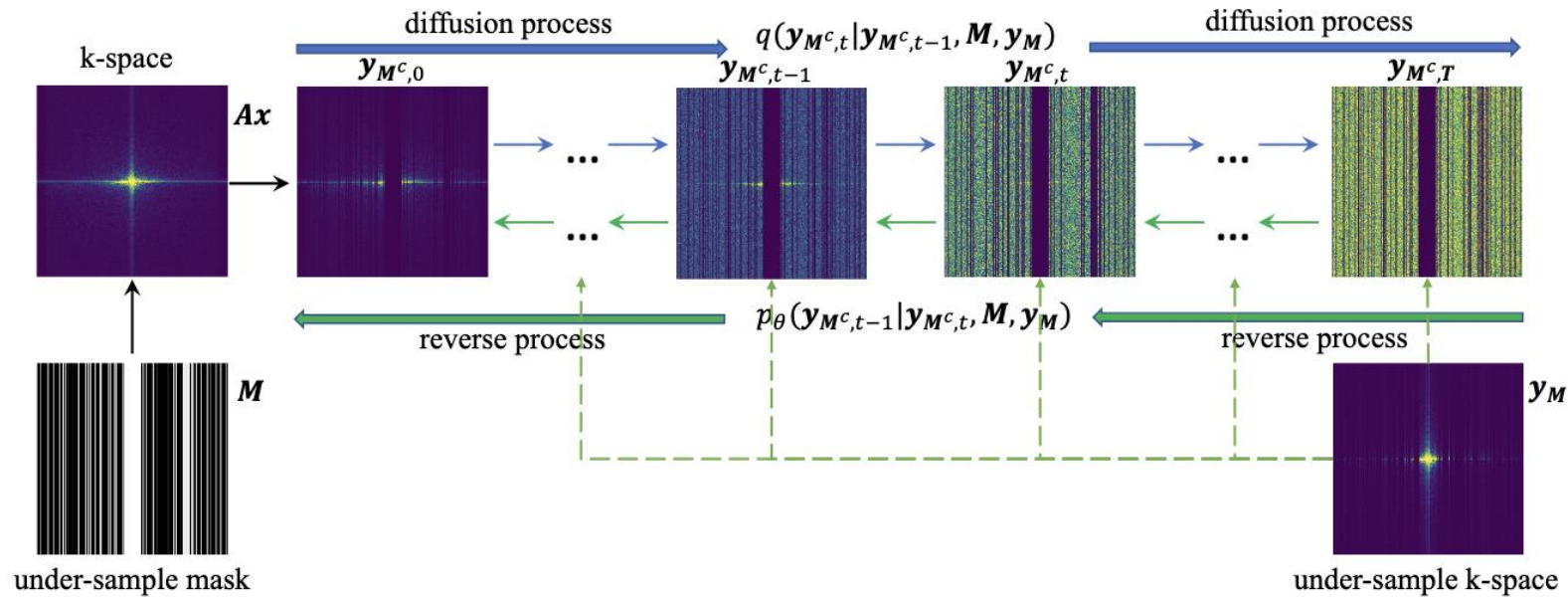
## IMAGES CAN BE RECONSTRUCTED USING AI



**Infinitely many solutions! Some more likely than others.**

# FIRST CONTRIBUTION: PROBABILISTIC MR RECONSTRUCTION

## State-of-the-art: MR Reconstruction based on Diffusion Models



Xie, Yutong, and Quanzheng Li. "Measurement-conditioned denoising diffusion probabilistic model for under-sampled medical image reconstruction." *International Conference on Medical Image Computing and Computer-Assisted Intervention*. Cham: Springer Nature Switzerland, 2022.

Best reconstructions, but **very slow inference** (~10 seconds *per slice*)

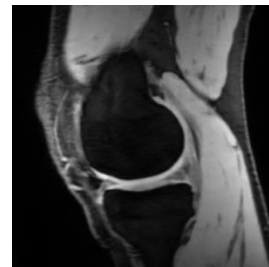
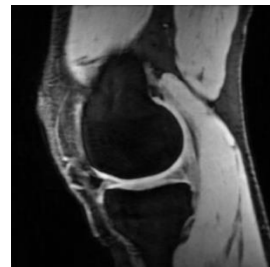
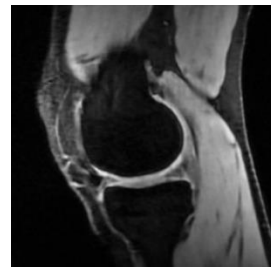
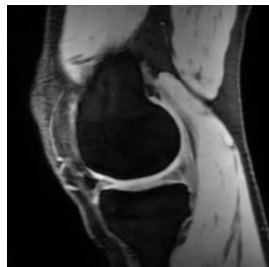
## OUR APPROACH IS BASED ON CONDITIONAL VAES

$x_u$



$p(x|x_u)$

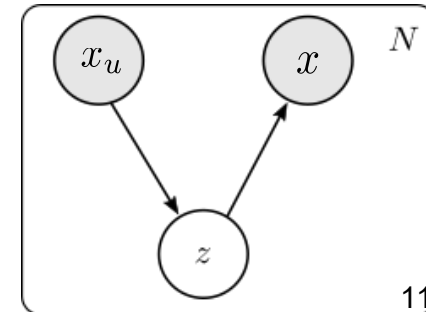
$x$



...

**Assumption of cVAE:** low-dimensional  $z$  explains all the variation

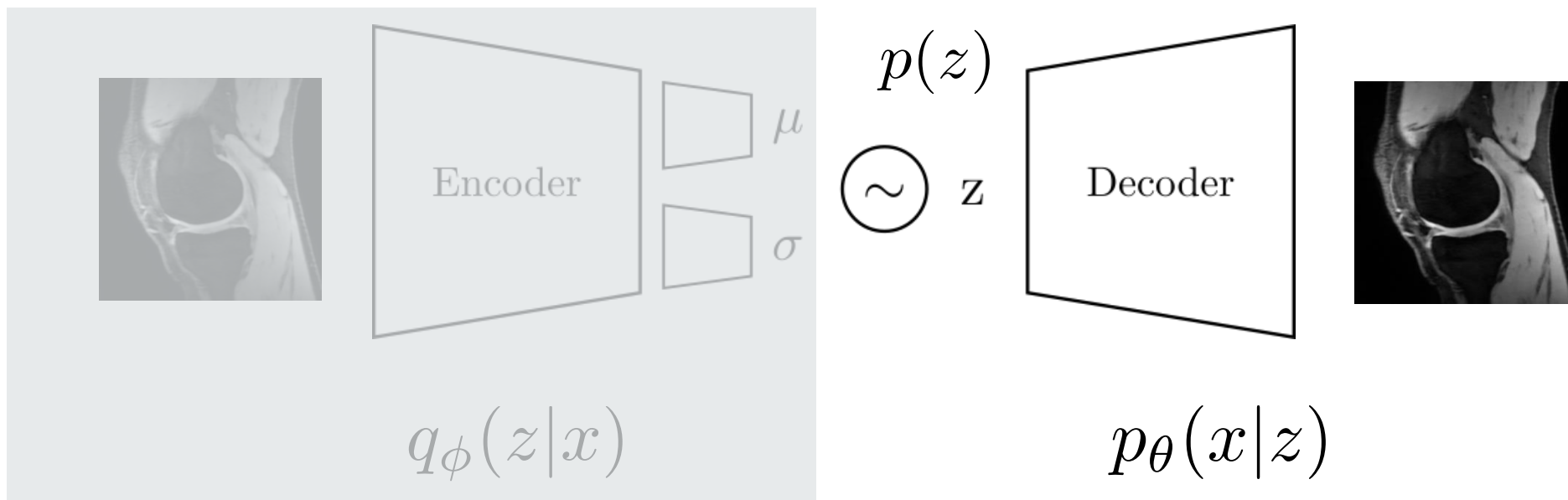
$$p(x|x_u) = \int p(x|z)p(z|x_u)dz$$





# VARIATIONAL AUTOENCODERS: A BRIEF INTRO

$$\ln p(x) \geq \mathbb{E}_{q_{\phi}(z|x)} [\ln p_{\theta}(x|z)] - \text{KL} [p(z) || q_{\phi}(z|x)]$$



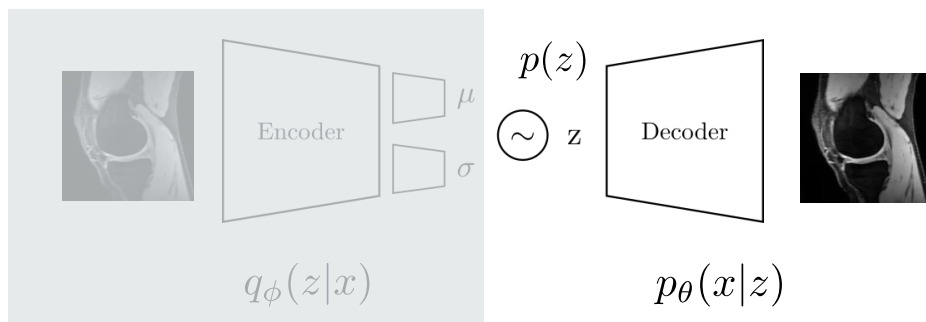
After training, discard posterior

# CONDITIONAL VARIATIONAL AUTOENCODERS

## VAE

$$p(s) = \int p(s|z)p(z)dz$$

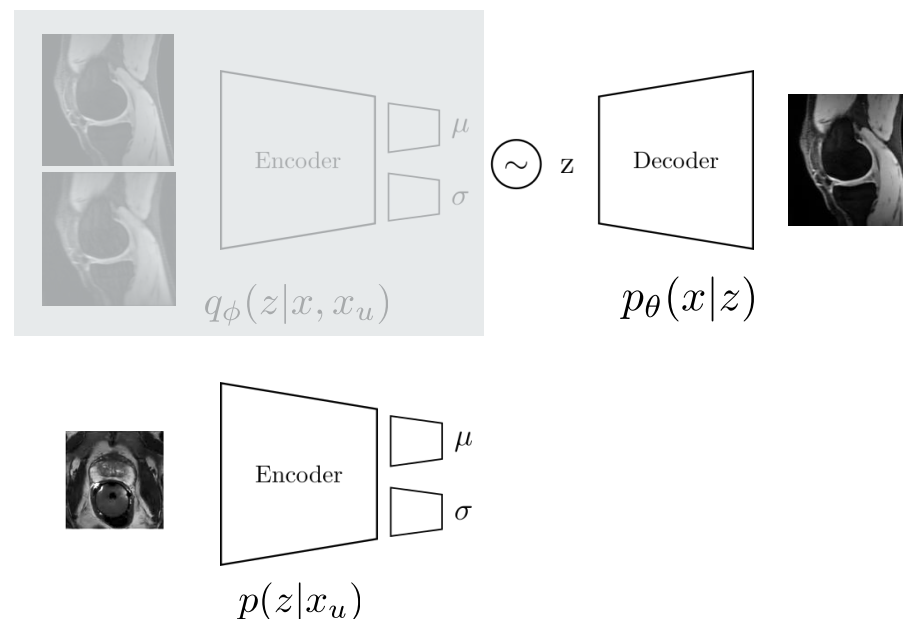
$$\ln p(x) \geq \mathbb{E}_{q_\phi(z|x)} [\ln p_\theta(x|z)] - \text{KL} [p(z) || q_\phi(z|x)]$$



## cVAE

$$p(x|\underline{x_u}) = \int p(x|z)p(z|\underline{x_u})dz$$

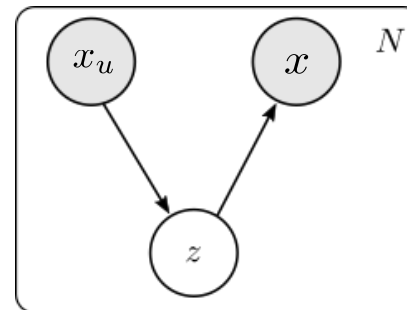
$$\ln p(x|\underline{x_u}) \geq \mathbb{E}_{q_\phi(z|x, \underline{x_u})} [\ln p_\theta(x|z)] - \text{KL} [p(\underline{z}|\underline{x_u}) || q_\phi(z|x, \underline{x_u})]$$



# FROM NORMAL CVAE TO HIERARCHICAL CVAE

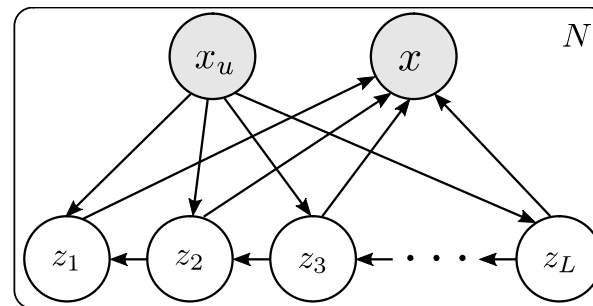
One level cVAE

$$p(x|x_u) = \int p(x|z)p(z|x_u)dz$$



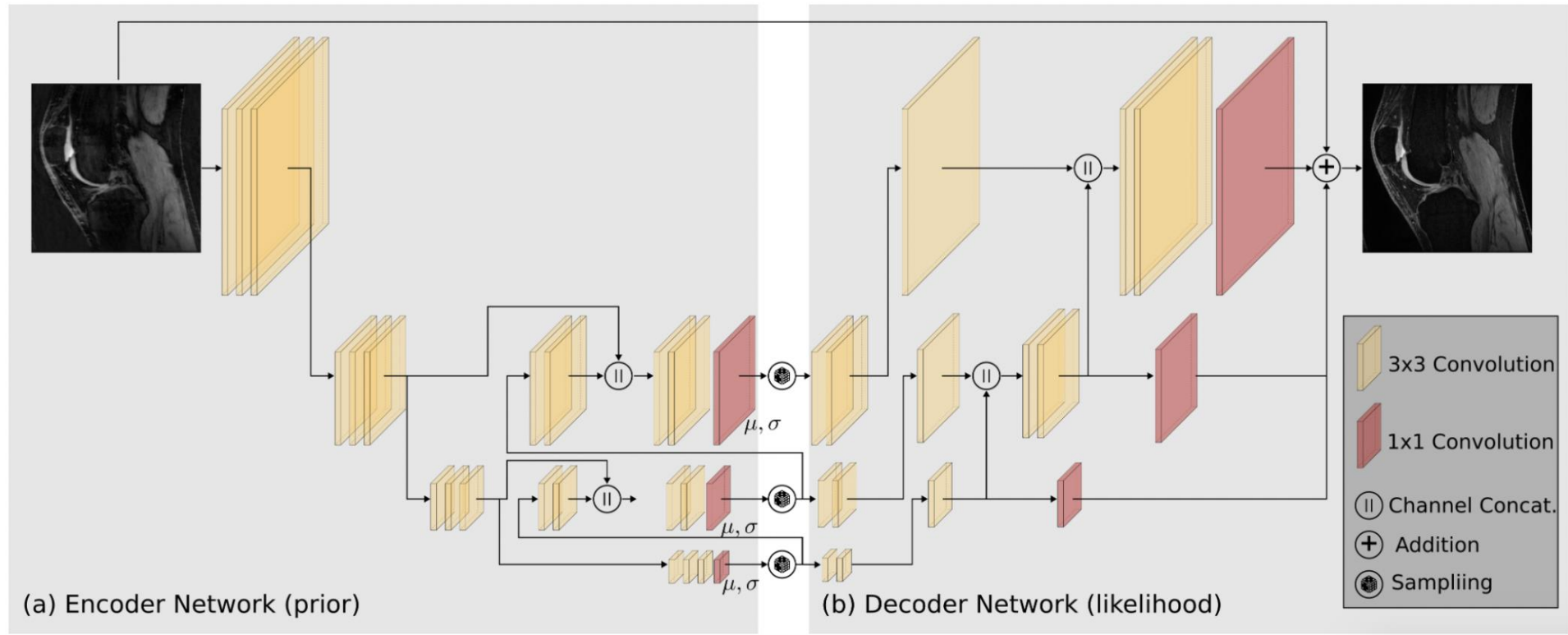
Hierarchical cVAE

$$p(x|x_u) = \int p(x|z_1, \dots, z_L)p(z_1|z_2, x_u) \cdots p(z_{L-1}|z_L, x_u)p(z_L|x_u)dz_1 \cdots dz_L$$

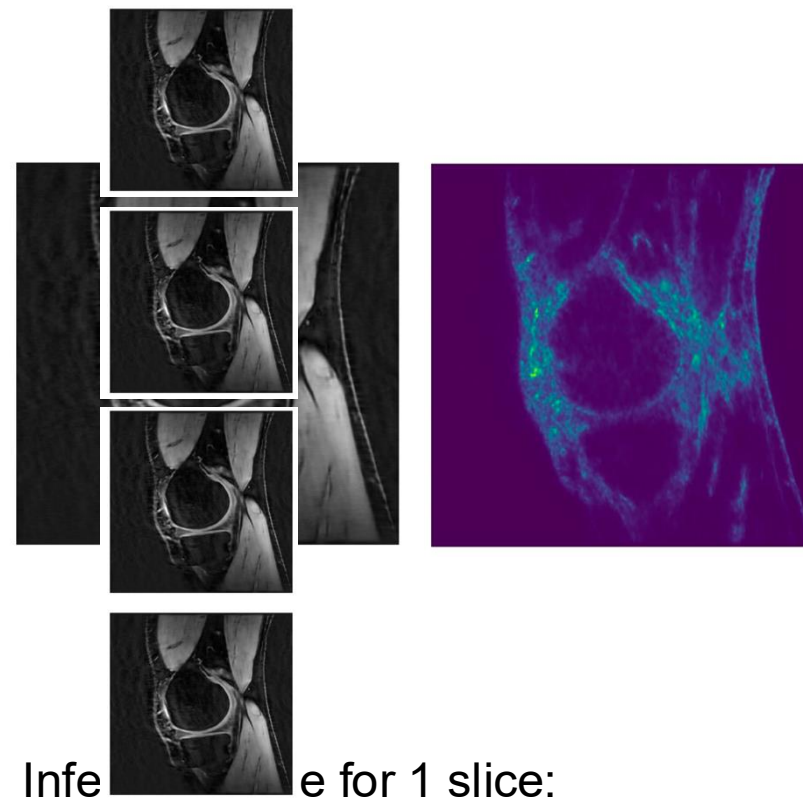
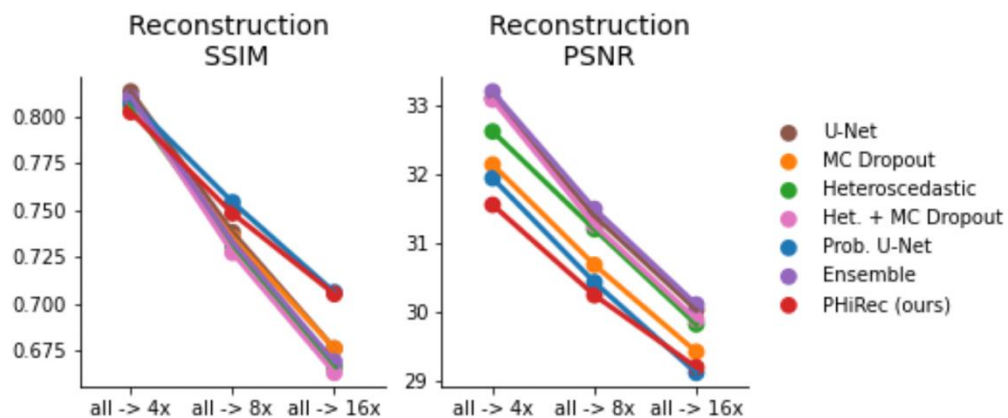
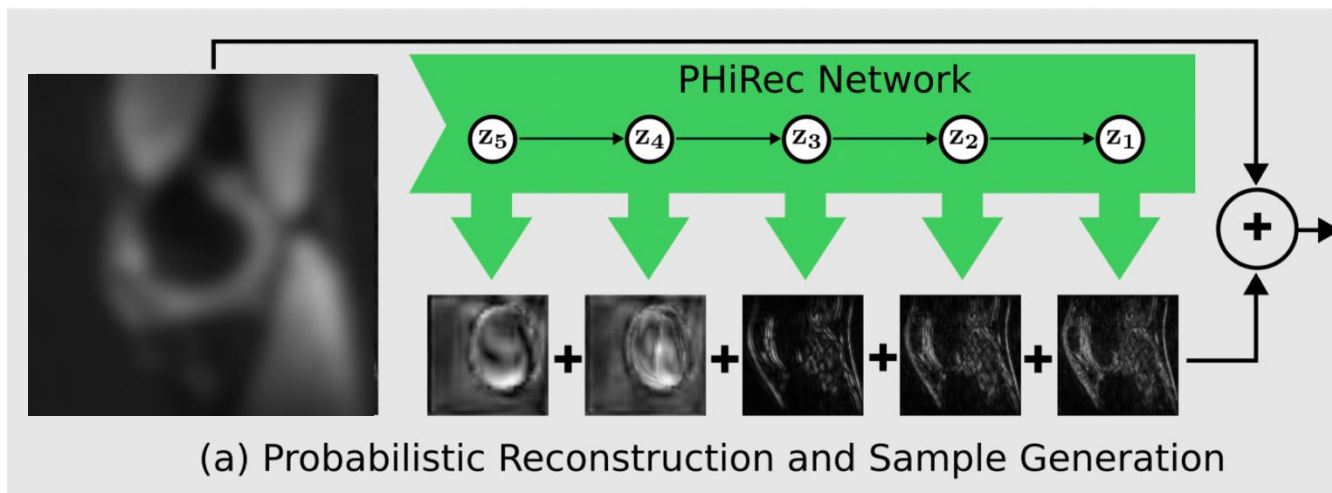




# PROBABILISTIC **HIERARCHICAL** RECONSTRUCTION (PHIREC)



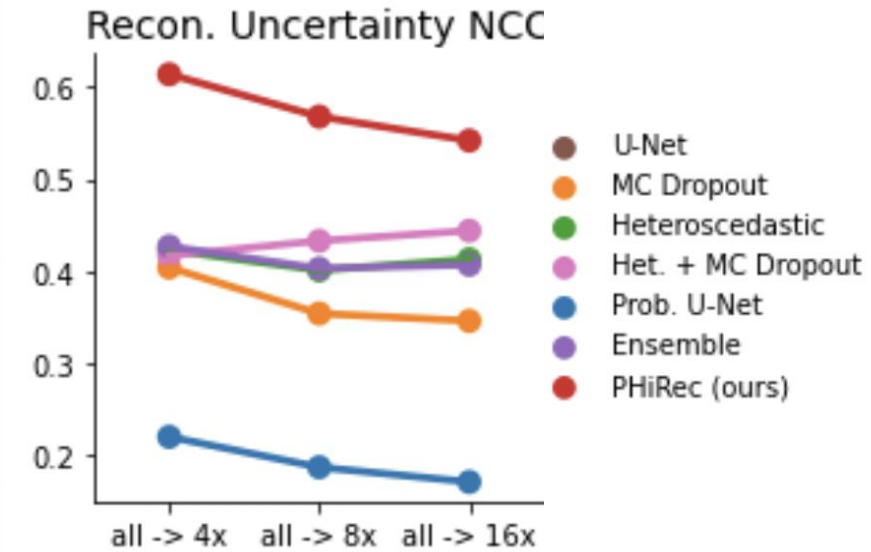
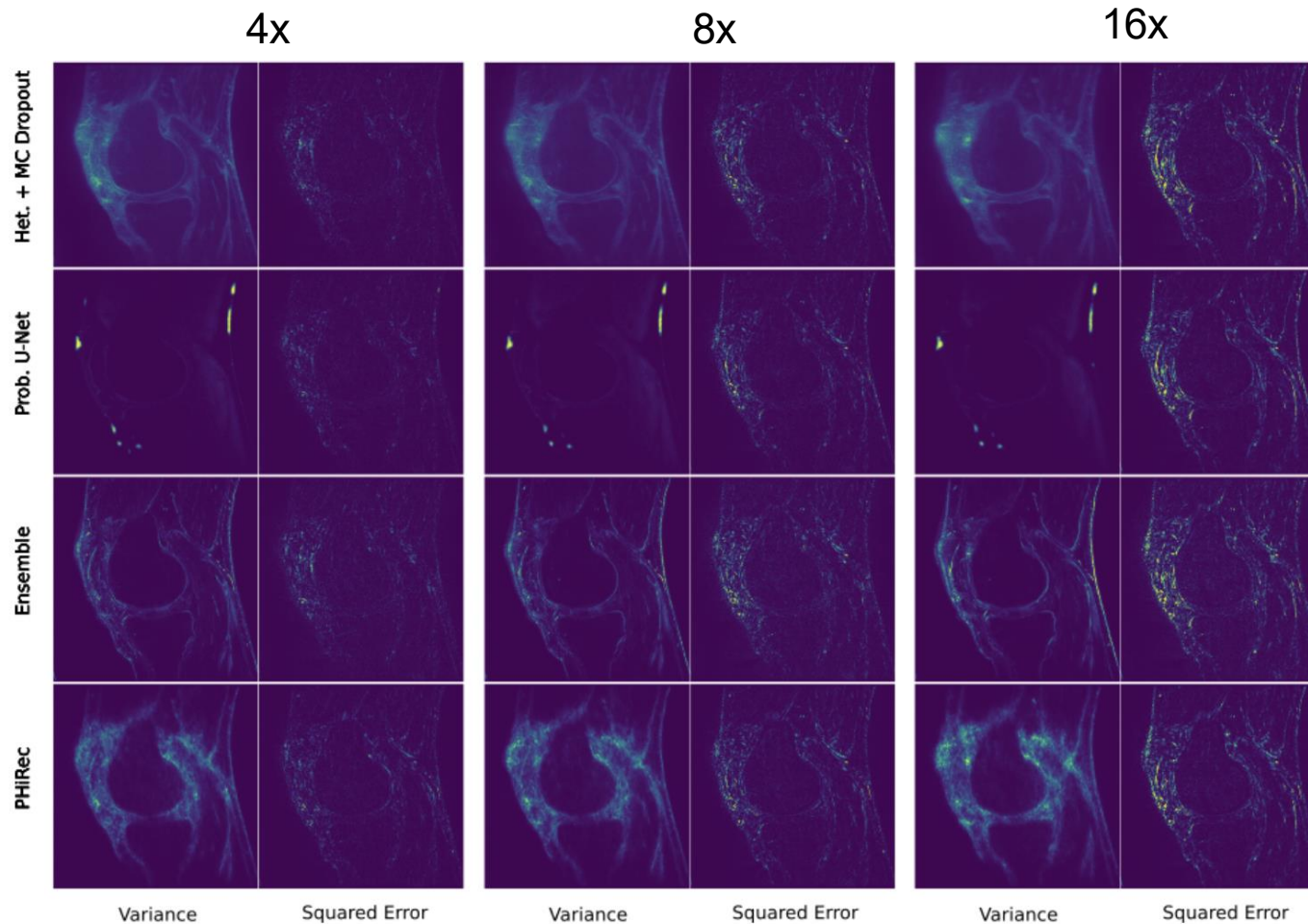
# PHIREC FOR ACCELERATED MR IMAGING AND UNCERTAINTY PROPAGATION



**PHiRec: 1ms**

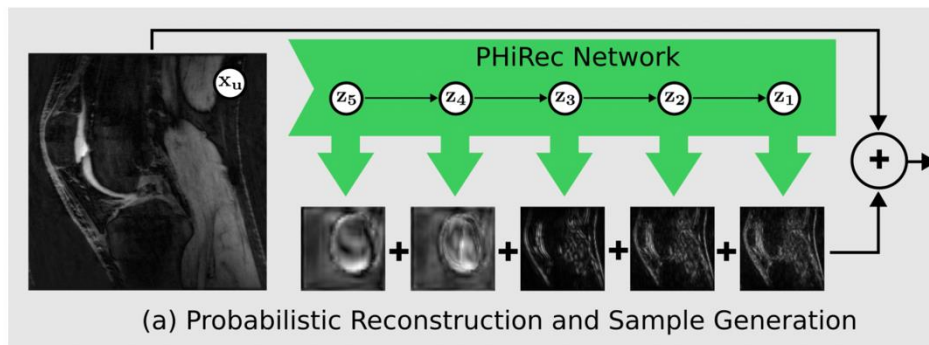
**Diffusion Model: ~10s**

# UNCERTAINTY QUANTIFICATION PERFORMANCE

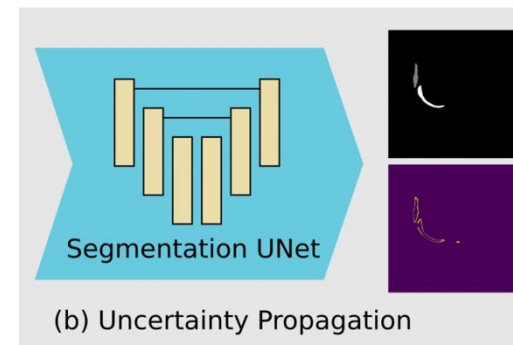
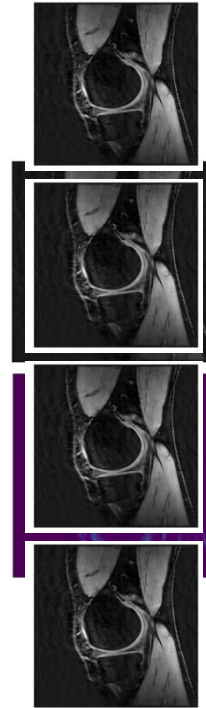




## PART 2: UNCERTAINTY PROPAGATION



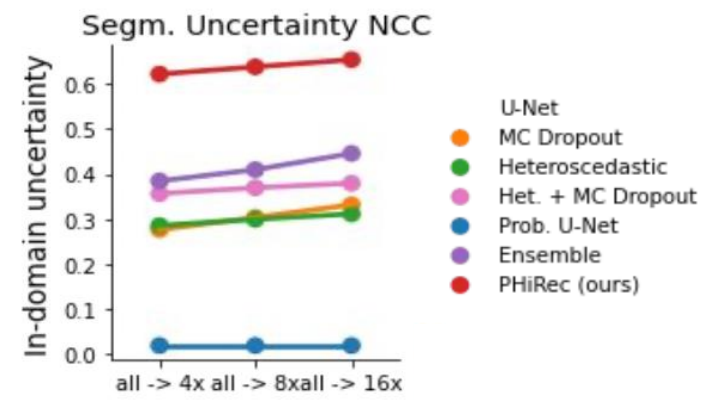
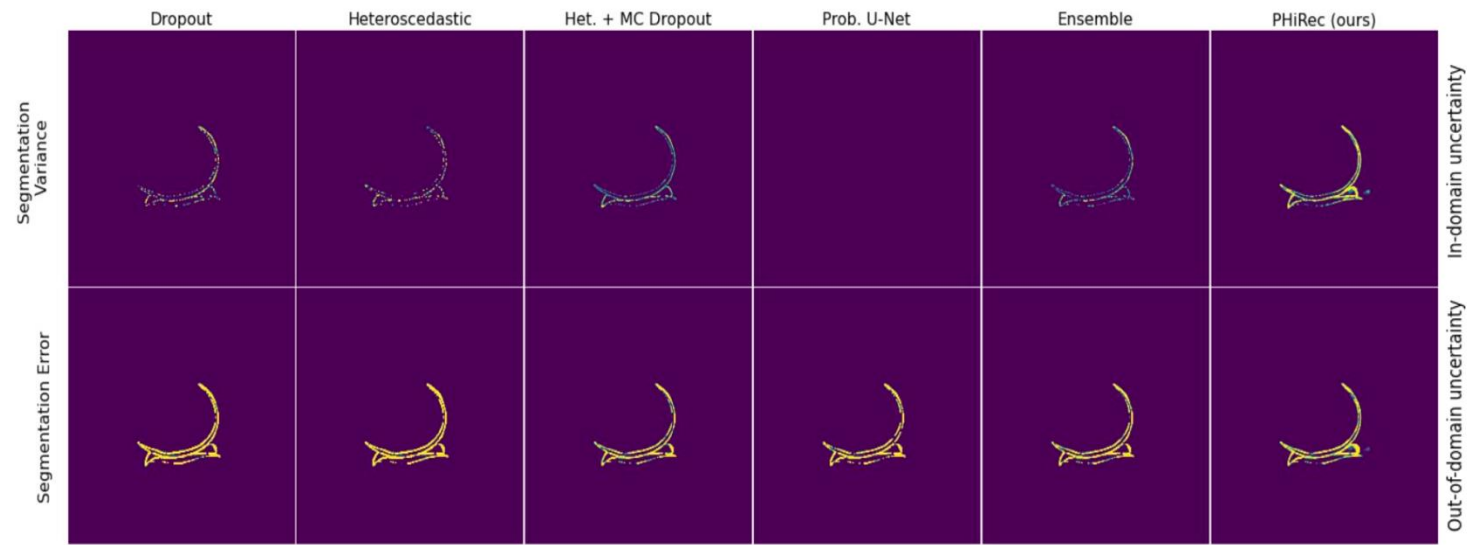
$$p(x|x_u)$$



$$f : x \mapsto s$$

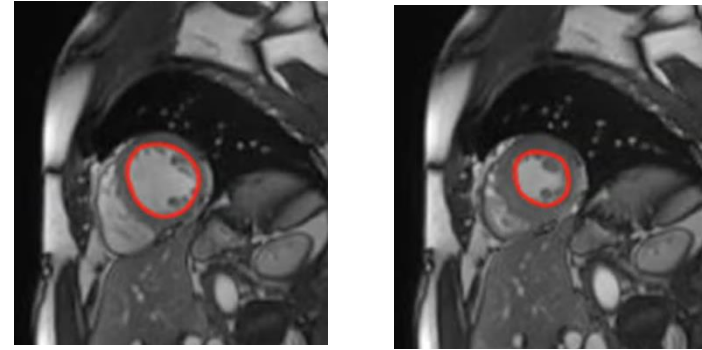
$$p(s|x_u) \approx \frac{1}{N} \sum_i^N \delta(s - f(X_i)), \quad X_i \sim p(x|x_u)$$

# RESULTS: UNCERTAINTY PROPAGATION



# PERSONALISED ADAPTIVE MR AQUISITIONS

**Goal:** Use patient-specific uncertainty to stop the scan early if the certainty is high enough for a downstream decision



$$\text{LVEF} = [(\text{End-Diastolic Volume} - \text{End-Systolic Volume}) / \text{End-Diastolic Volume}]$$

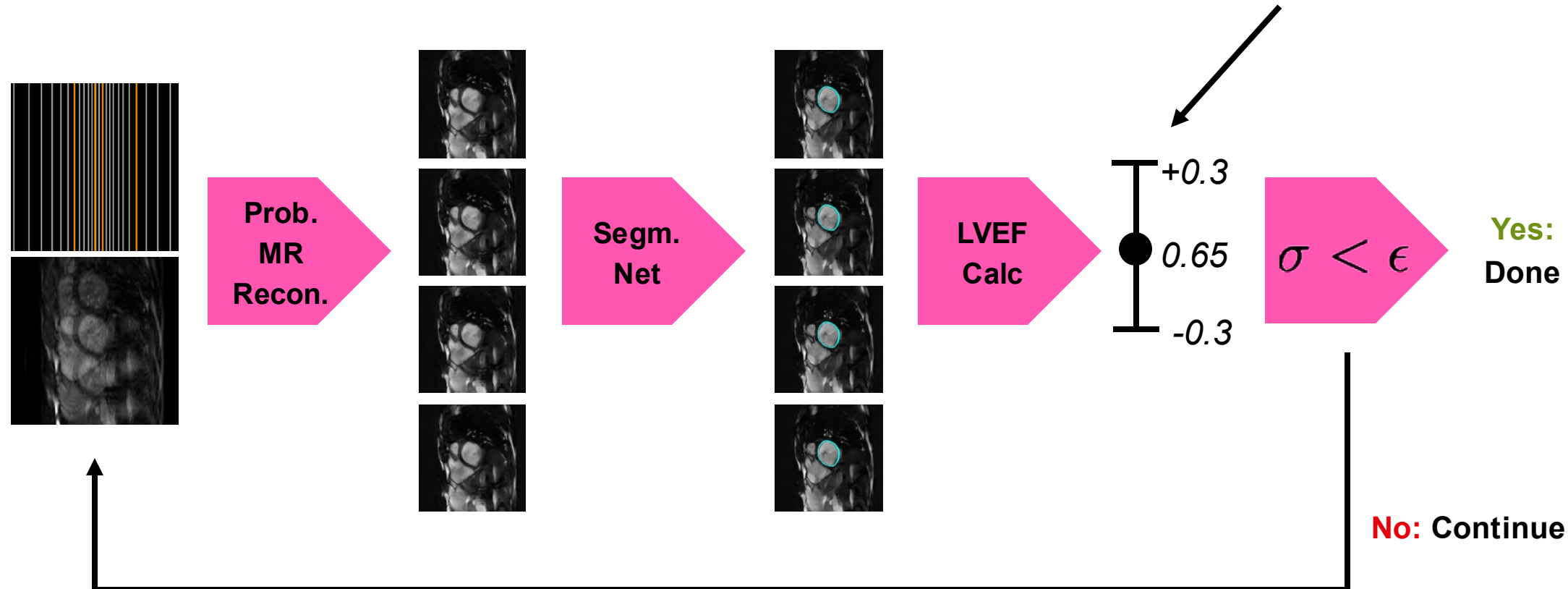


**Alice:** Young healthy subject with normal cardiac anatomy. Faster acceleration possible.



**Bob:** Unusual Cardiac Anatomy, irregular breathing. Only low acceleration possible.

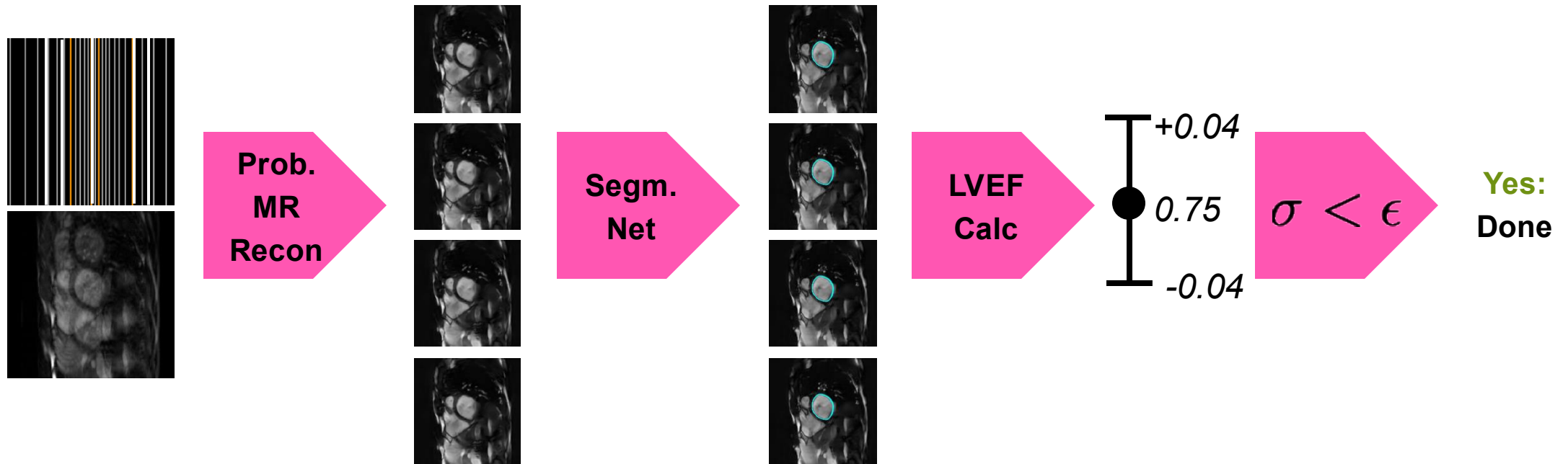
# UNCERTAINTY-GUIDED MR ACQUISITION



**Paul Fischer**, Jan Nikolas Morshuis, Thomas Küstner, Christian F Baumgartner, CUTE-MRI: Conformalized Uncertainty-based framework for Time-adaptive MRI, Elsevier Medical Image Analysis (under review)

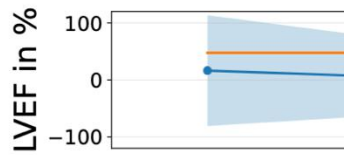


# UNCERTAINTY-GUIDED MR ACQUISITION



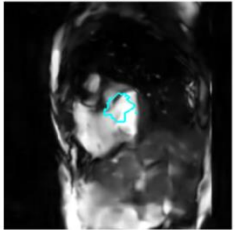
**Paul Fischer**, Jan Nikolas Morshuis, Thomas Küstner, Christian F Baumgartner, CUTE-MRI: Conformalized Uncertainty-based framework for Time-adaptive MRI, Elsevier Medical Image Analysis (under review)

## CASE EXAMPLE: “EASY” CASE

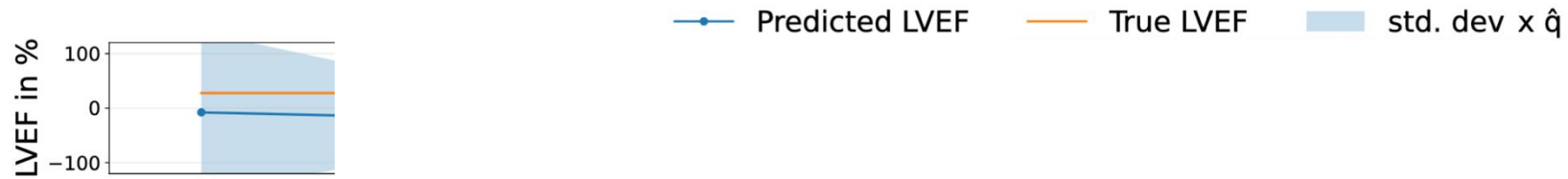


—●— Predicted LVEF    — True LVEF    ■ std. dev  $\times \hat{q}$

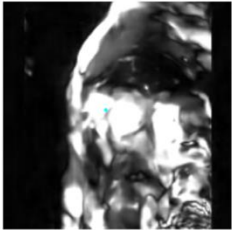
32x

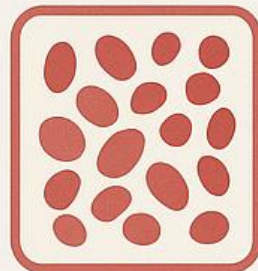
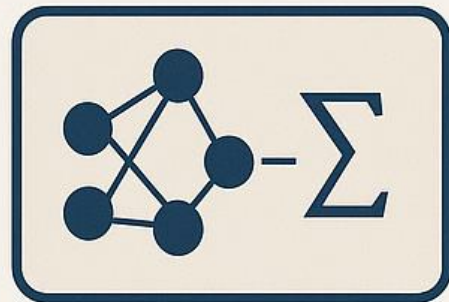
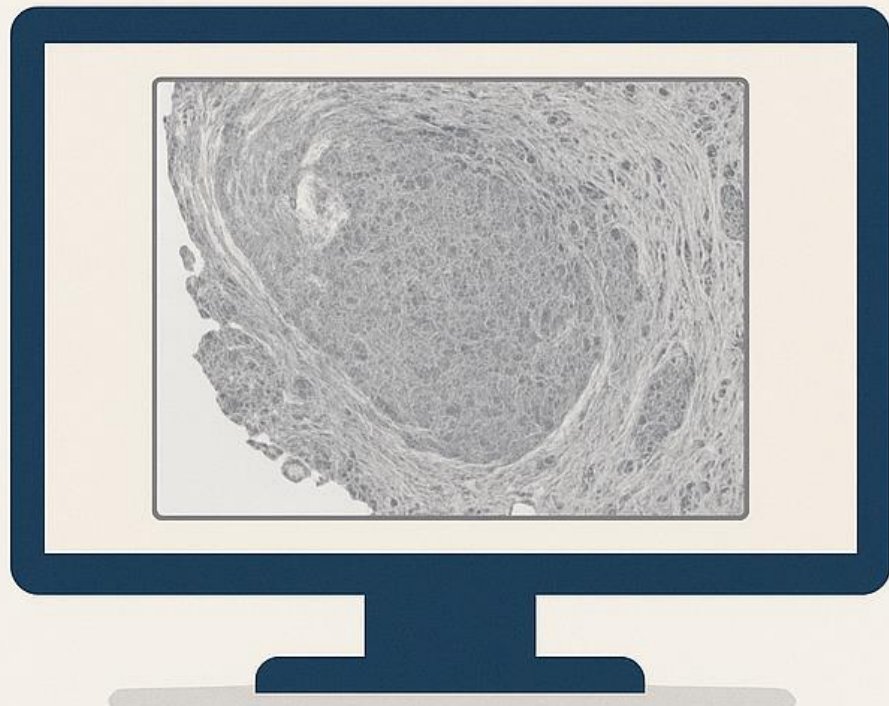


## CASE EXAMPLE: “DIFFICULT CASE”



32x





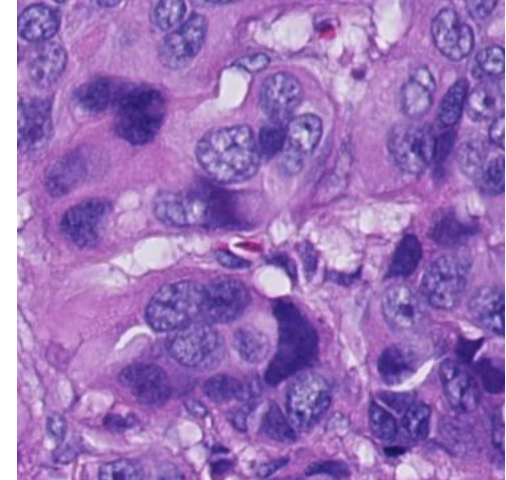
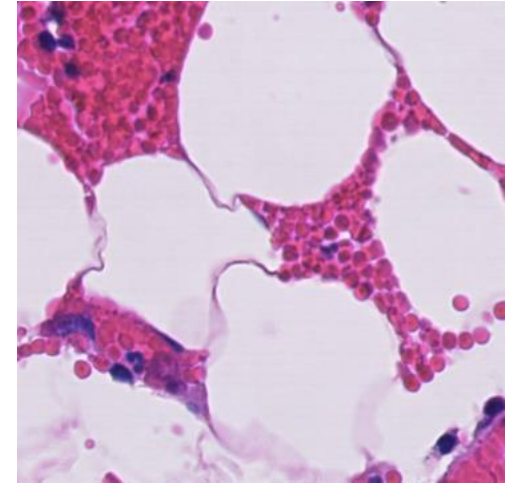
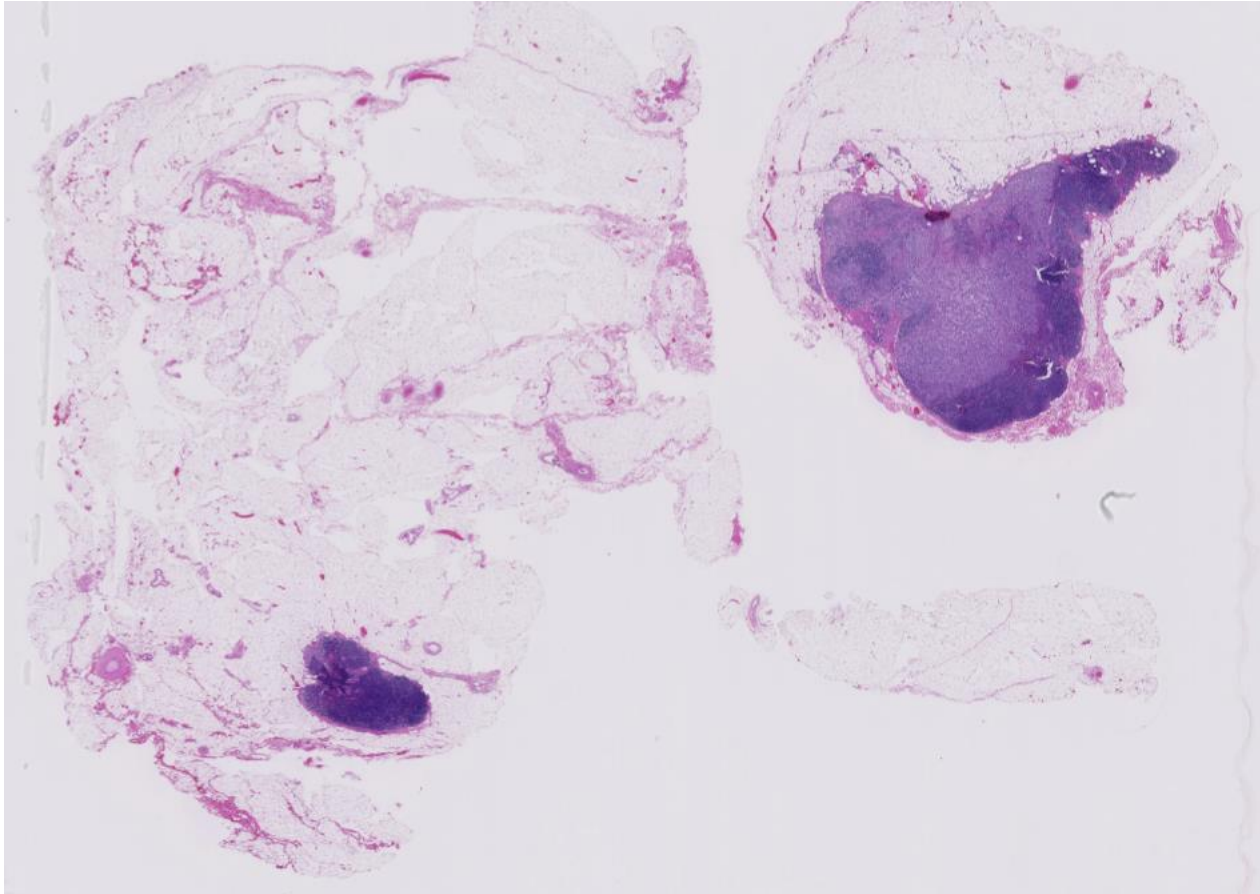
## EXPLAINABLE WHOLE SLIDE IMAGE DIAGNOSIS WITH AI



**Susu Sun**  
PhD Student



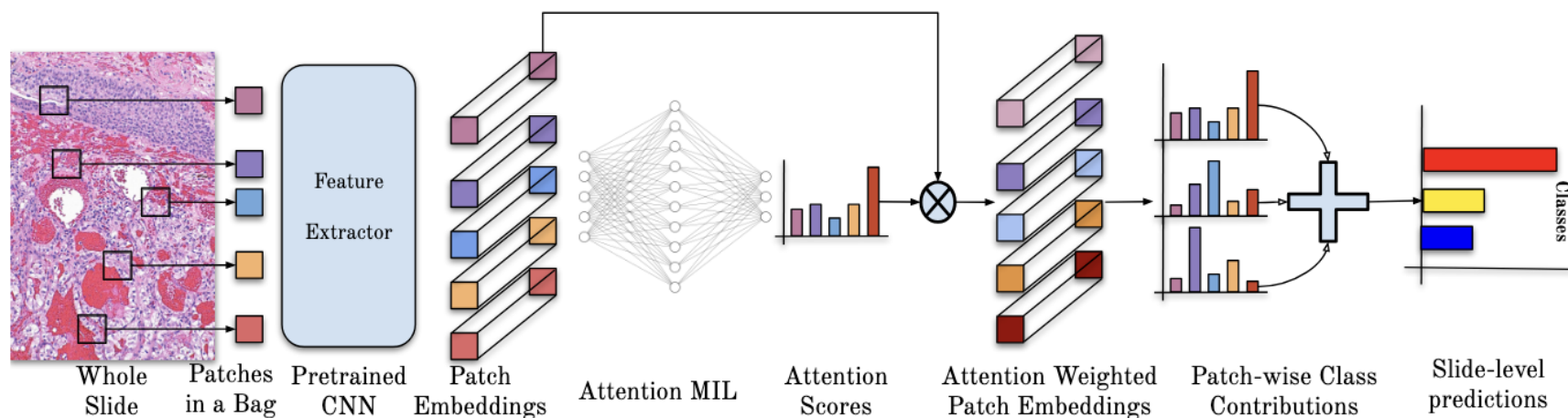
## WHOLE SLIDE IMAGES (WSI)



**Challenge for AI: WSI are huge (on the order of 100'000 x 100'000 pixels)**

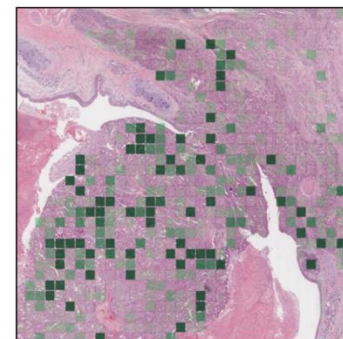
# PRIOR STATE-OF-THE-ART

## Multi-instance Learning (MIL)



### Problems:

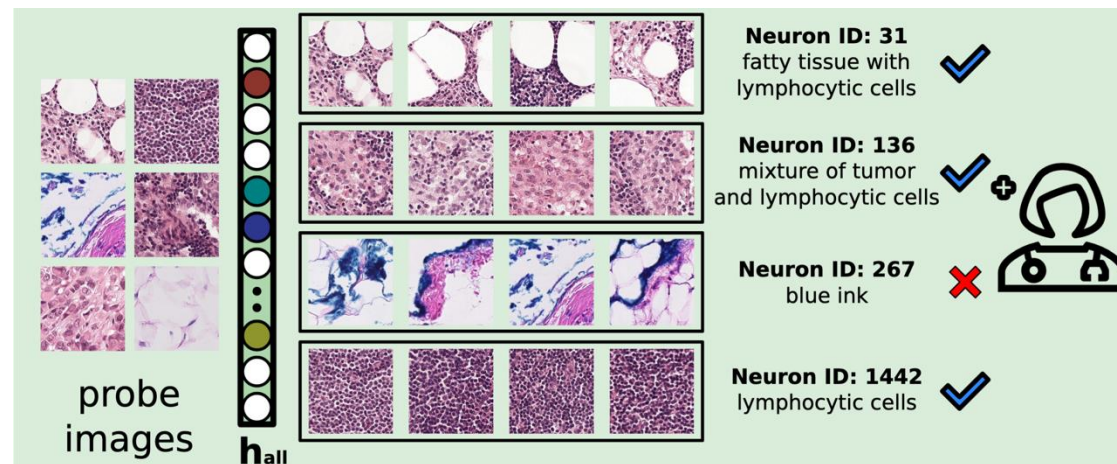
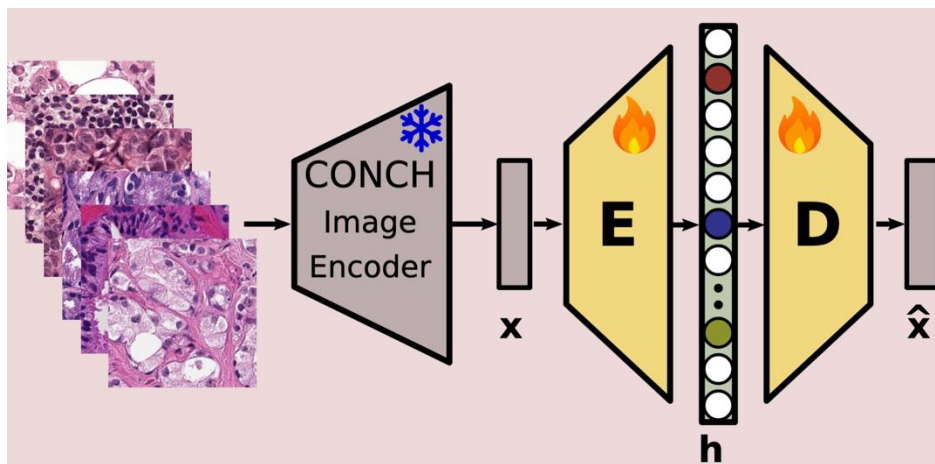
- Knowing *where* is not the same as knowing *why*
- Attention maps are known to not accurately reflect the model's decision



Attention Maps

Javed, S. A., Juyal, D., Padigela, H., Taylor-Weiner, A., Yu, L., & Prakash, A. (2022). Additive mil: Intrinsically interpretable multiple instance learning for pathology. *Advances in Neural Information Processing Systems*, 35, 20689-20702.

## OUR IDEA: FIRST STEP - DISCOVER AND NAME CONCEPTS



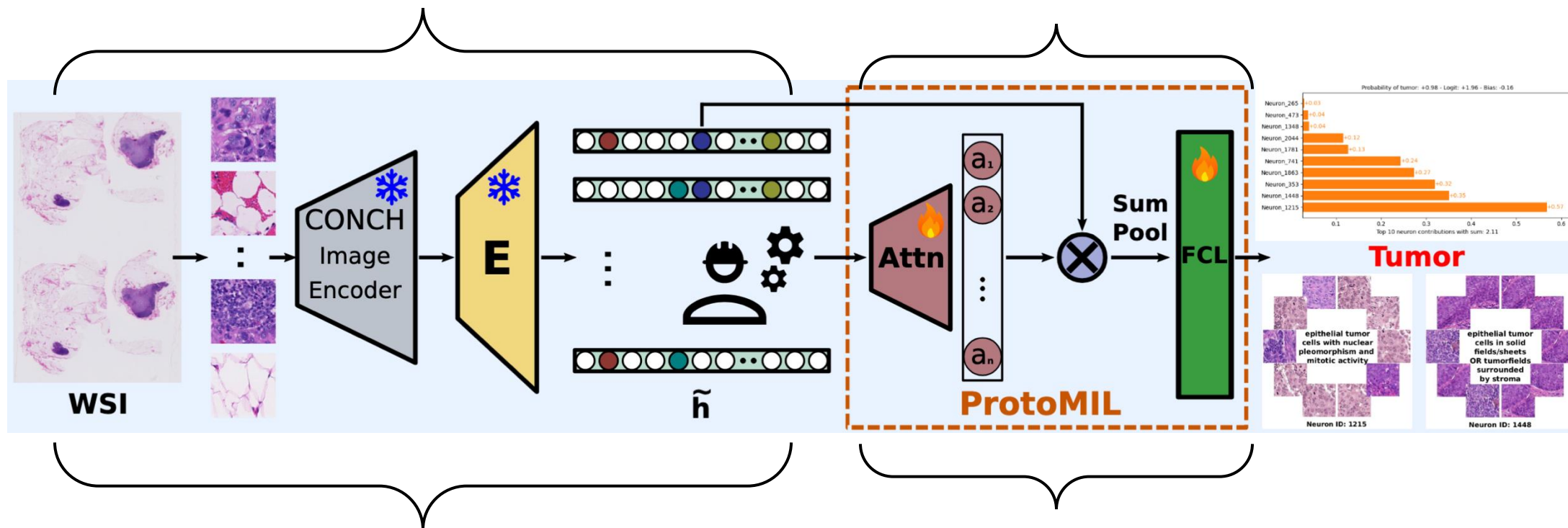
A **sparse autoencoder** is used to compress WSI patches to just a few informative neurons

We check what type of patch activates each neuron the most and ask a pathologist to name them

**Susu Sun**, Dominique van Midden, Geert Litjens, and Christian F. Baumgartner. "Prototype-Based Multiple Instance Learning for Gigapixel Whole Slide Image Classification." *Proc. MICCAI* (2025).



## SECOND STEP: ENCODE TRAINING INTO NEURONS AND TRAIN A MIL APPROACH ON THEM

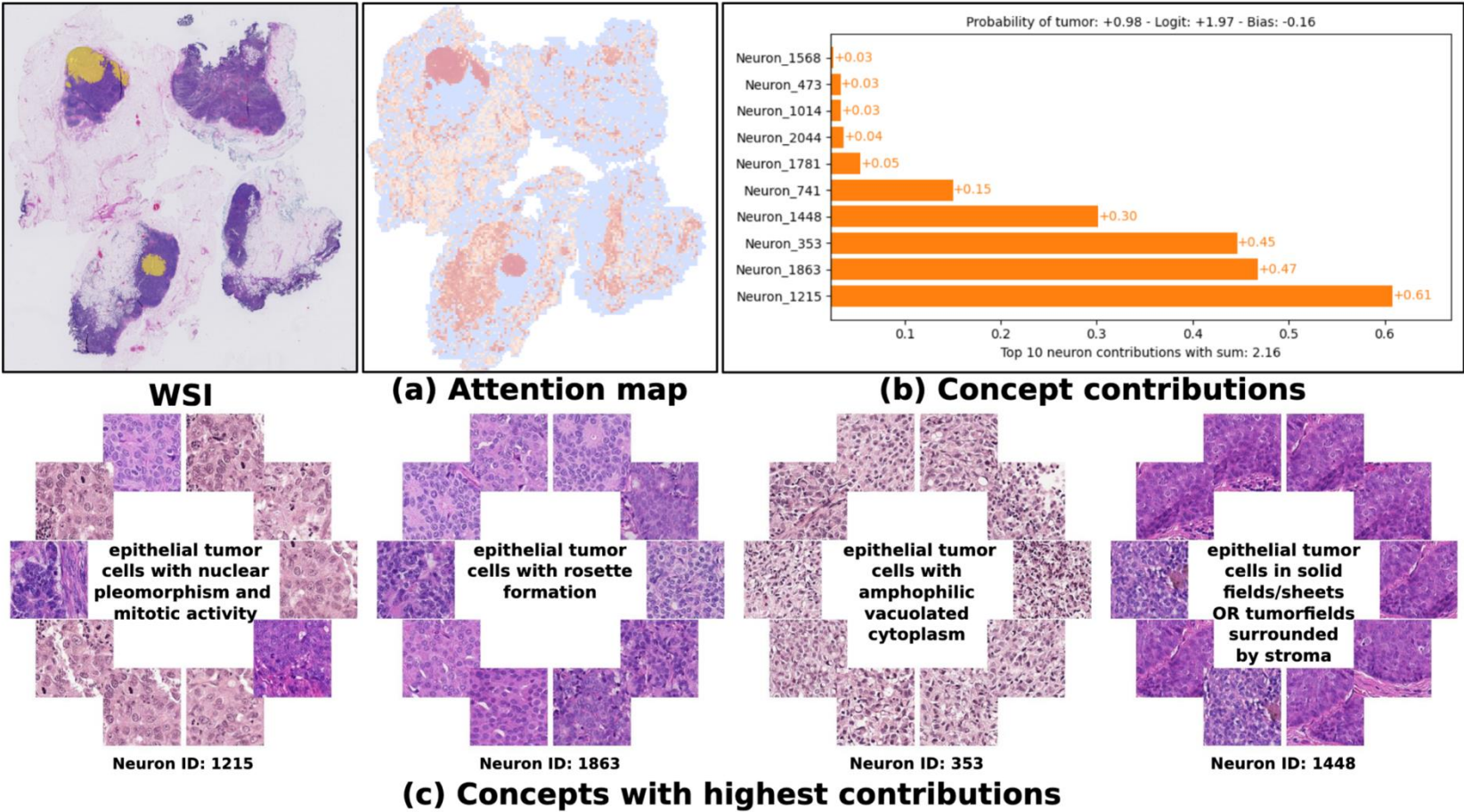


Applying the encoder part of the sparse autoencoder from before

Use a very simple MIL model for classification



# OUTPUT OF OUR PROPOSED MODEL



# REMOVING UNWANTED SHORTCUT LEARNING

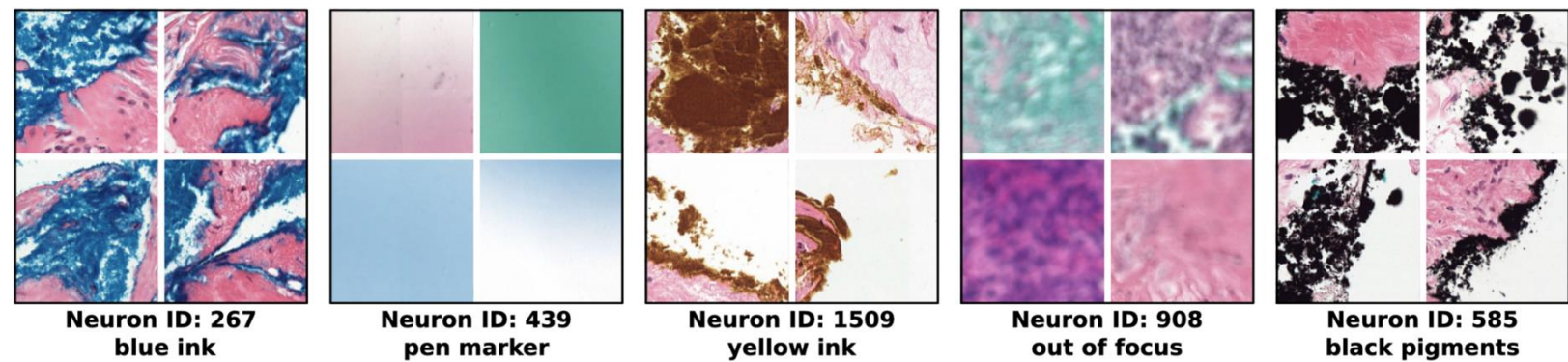


Table 1. Classification performance measured by Accuracy and AUC.

| Model                          | Camelyon16 |       | PANDA |       |
|--------------------------------|------------|-------|-------|-------|
|                                | Acc.       | AUC   | Acc.  | AUC   |
| ABMIL (image)                  | 0.922      | 0.908 | 0.892 | 0.953 |
| CLAM (image)                   | 0.915      | 0.966 | 0.884 | 0.979 |
| TransMIL (image)               | 0.938      | 0.950 | 0.939 | 0.977 |
| AdditiveMIL (image)            | 0.875      | 0.883 | 0.905 | 0.958 |
| ProtoMIL (concept)             | 0.907      | 0.918 | 0.916 | 0.970 |
| ProtoMIL (intervened concepts) | 0.926      | 0.913 | 0.916 | 0.964 |

# THANK YOU FOR YOUR ATTENTION



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PhD Student



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University Hospital Tübingen



**Prof. Geert Litjens**

Radboud University Medical Center